

JOHN ADAMS INSTITUTE FOR ACCELERATOR SCIENCE
DEPARTMENT OF PHYSICS



UNIVERSITY OF
OXFORD

PAMELA Overview

Suzie Sheehy

International Workshop on FFAG Accelerators (FFAG '10)
Kyoto University Research Reactor Institute, Osaka, Japan



Φ xford
physics

Outline

- Overview of PAMELA project
- Clinical requirements
- Injection and ion sources
- Lattice design & performance
- Magnet design
- RF design
- Beam transport & gantry
- Summary

Overview

PAMELA: Particle Accelerator for MEDical Applications

One of 3 work packages of the CONFORM collaboration

Aim: “to design a prototype proton/carbon ion ns-FFAG accelerator for charged particle therapy”

Other work packages:

- EMMA (Electron Model of Many Applications)
- Applications (ADSR, particle therapy, radioisotopes etc...)

Collaboration in UK

Oxford (JAI, Gray, PTCRi)

John Cobb , Bleddyn Jones, Ken Peach,
Suzie Sheehy, Holger Witte, Takeichiro
Yokoi, Mark Hill, Boris Vojnovic + others

Brunel University

Richard Fenning, Akram Khan

Imperial College London

Morteza Aslaninajad, Matt Easton,
Jaroslaw Pasternak, Juergen Pozimski

STFC/ASTeC/RAL, STFC/DL

Elwyn Baynham, Neil Bliss, Rob
Edgecock, Ian Gardner, David Kelliher,
Neil Marks, Shinji Machida, Peter
McIntosh, Chris Prior, Susan Smith

Lattice Design



Injection



Extraction



Magnet Design



Medical Requirements



RF



Gantry



Beam transport



Front end



Injection line



Ion sources



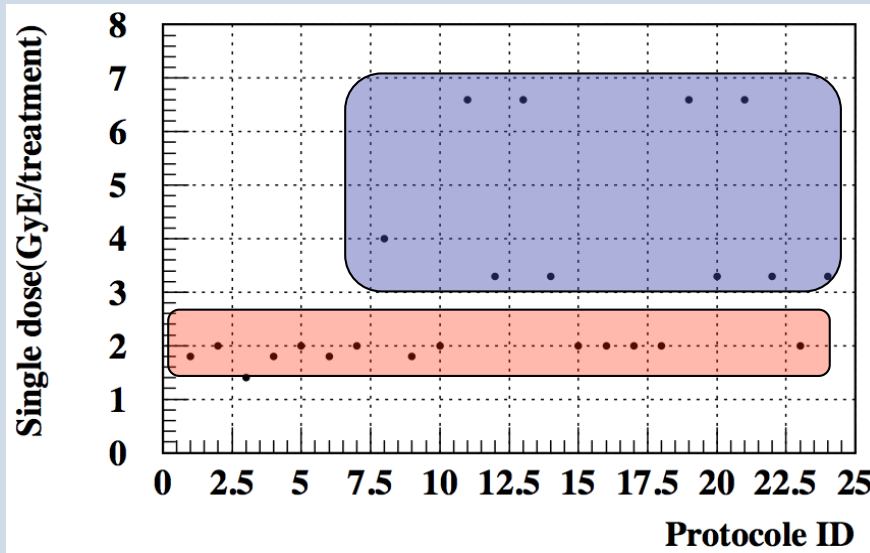
Engineering solutions



Doses for treatment

- Low radiosensitive tissue**
(lung, liver etc)
- high radiosensitive tissue**
(brain, perif. of digestive canal etc)

Proton



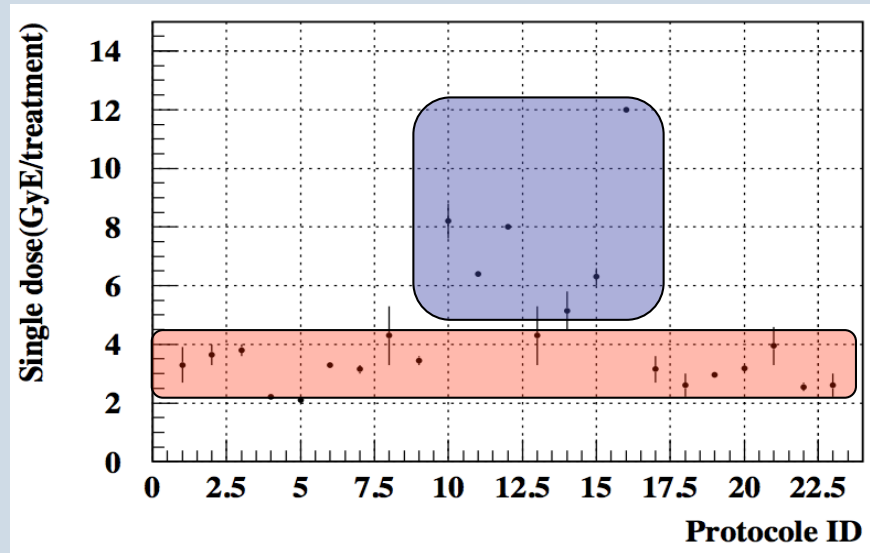
Courtesy of T.Okumura (Tsukuba univ.)

Proton: 1~7GyE (Tsukuba Univ, Japan)

radio-sensitive tissues : **1 - 2 GyE**

non radio-sensitive tissues : **3 - 7 GyE**

Carbon



Report by ANTM (Japan,2002)

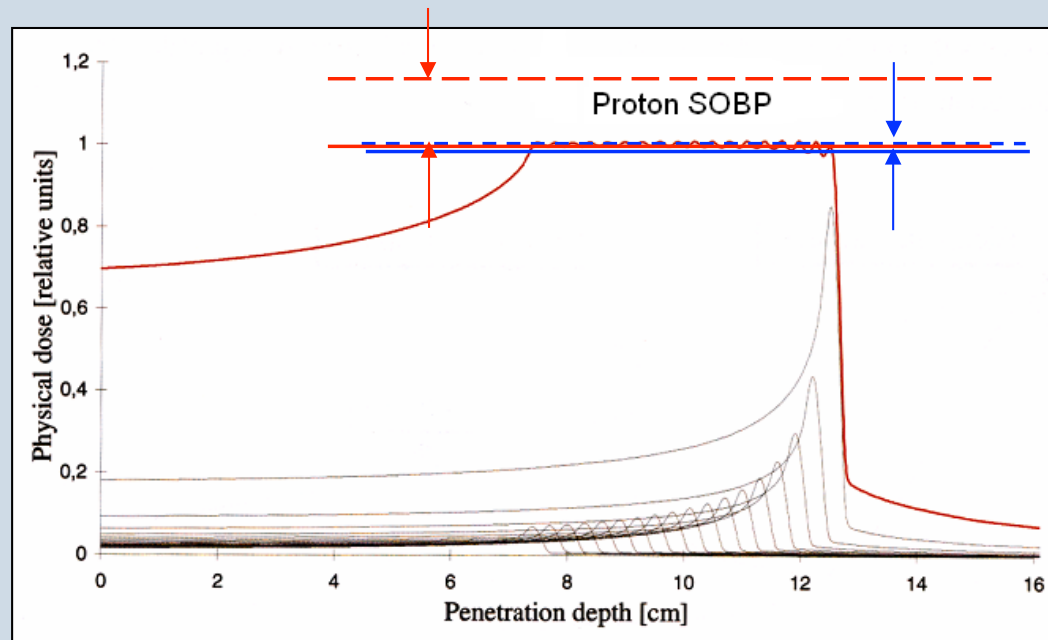
Carbon: 2~12GyE (NIRS,Japan)

radio-sensitive tissues : **2 - 4 GyE**

non radio-sensitive tissues : **4 - 12 GyE**

Clinical Requirements – dose control

In dose field formation: **uniformity** and **tolerance** are important



Uniformity => Stability
“deviation of local dose from average dose”

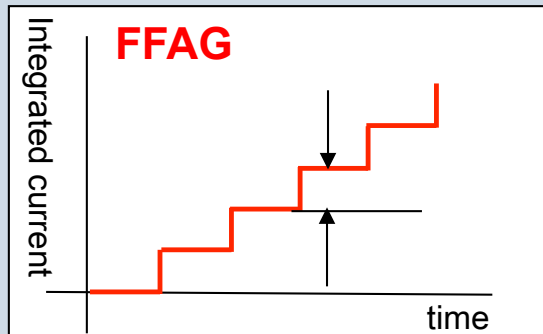
Tolerance => Tunability
“deviation of average dose from prescribed dose”

** SOBP is not necessarily the ideal dose field in spot scanning

Uniformity : <2%

Tolerance : <5% (existing facilities already achieved <2%)

Clinical Requirements



Step size controls dose (injection)

To achieve Intensity Modulated Particle Therapy:

- multi-beam painting with small bunch intensity
- simple system, but high repetition rate

Rescanning: ~ 5 may be needed to achieve good uniformity (multi-bunch)

Proton: $0.2\text{nA/GyE} \Rightarrow 0.05\text{nA} \sim 0.4(1.4)\text{nA}$ (Carbon divide by 36) for 1L

Beam position reproducibility of 0.2 mm (achieved at PSI)

Scanning speed > 100 Voxel/sec

Beam size 4 mm – 10 mm FWHM (variable)

Facility lifetime > 20 years -> Flexibility is crucial!

Accelerator Challenges

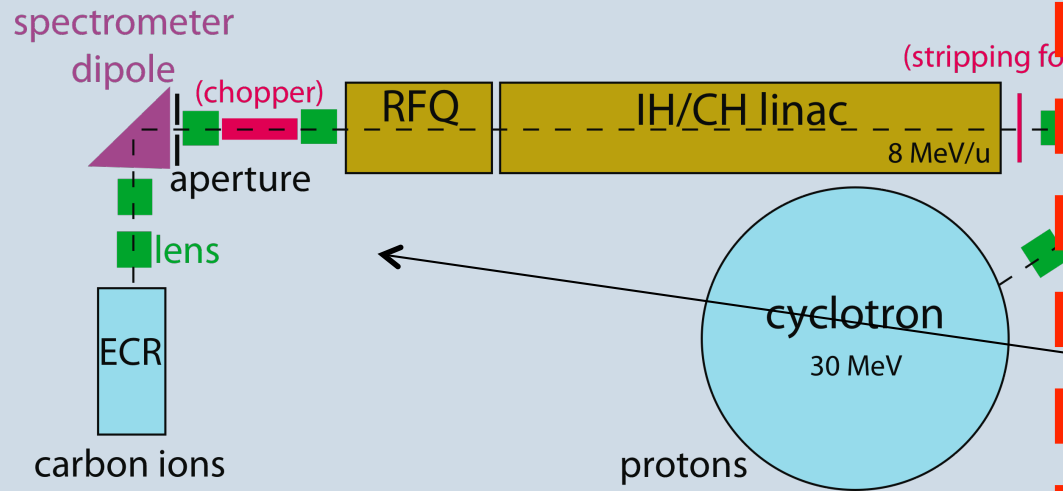
Clinical requirements translate to:

- Variable energy extraction
- 1 kHz repetition rate
- Small accelerator footprint

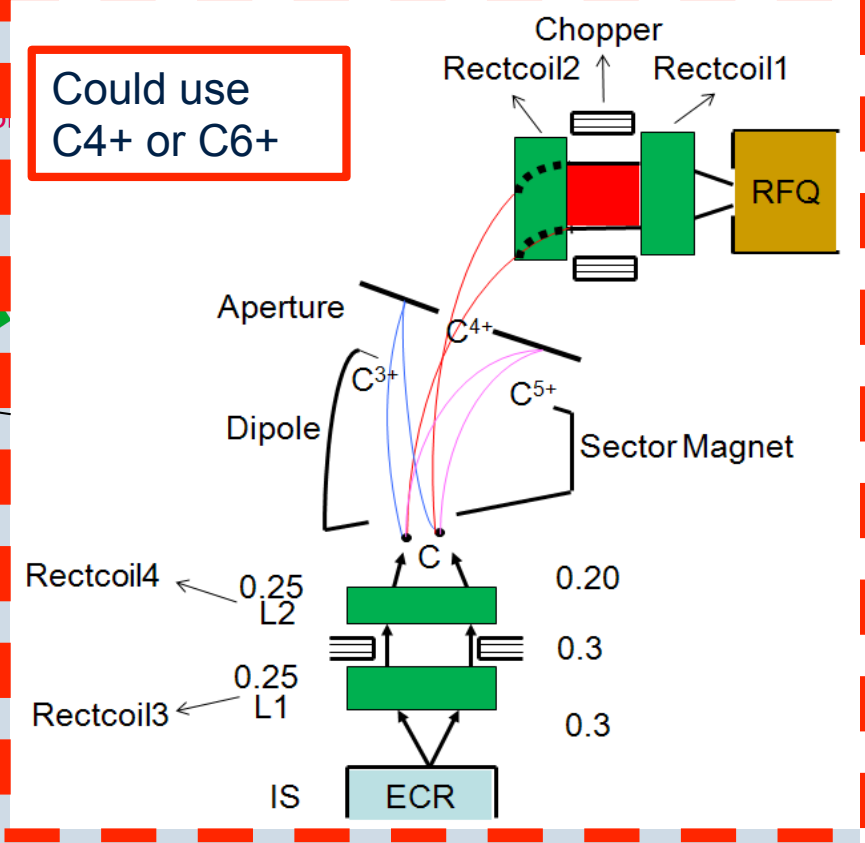
We also want:

- Small(ish) aperture (scaling FFAG > 1m!)
- Avoid crossing harmful resonances (linear ns-FFAG)

Injector and Ion Sources



Could use C4+ or C6+



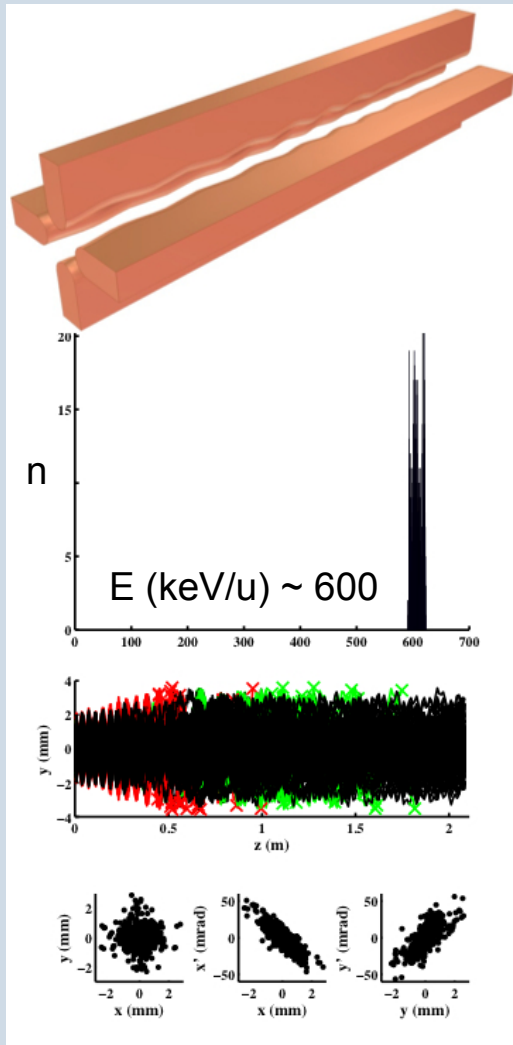
ECR: ECRIS

Hypernanogun

We need 0.6 μA Carbon 6⁺.

ECRIS can produce 1 μA Carbon 6⁺ => use this directly!

RFQ and IH/CH linac



RFQ

Transmission: 97%
 Mean energy: ~600 keV/u
 Frequency: 280 MHz
 Length: 3.56m / 800 cells

Based on scaled version of FETS design

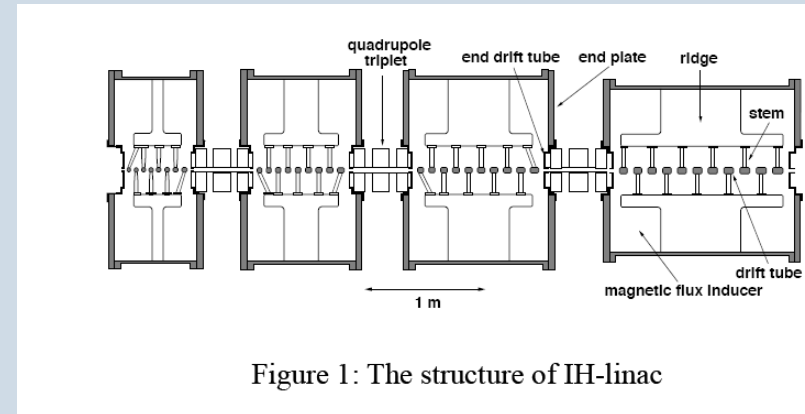
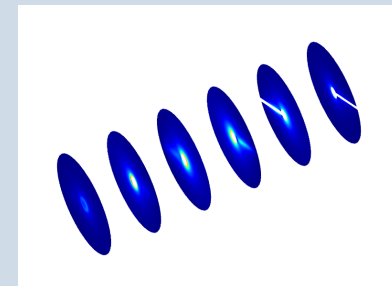
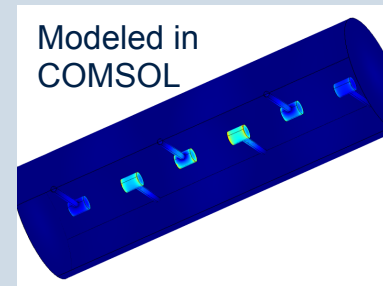


Figure 1: The structure of IH-linac



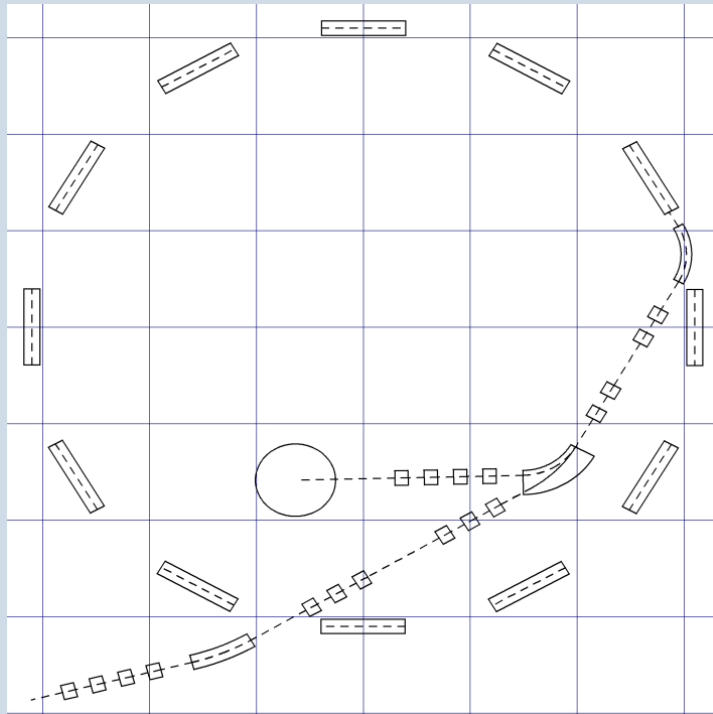
Drift tubes mounted on alternating sides.

- Pi mode -> enhanced transit-time factor
- Compact drift tube -> very small capacitance
- Higher Shunt Impedance

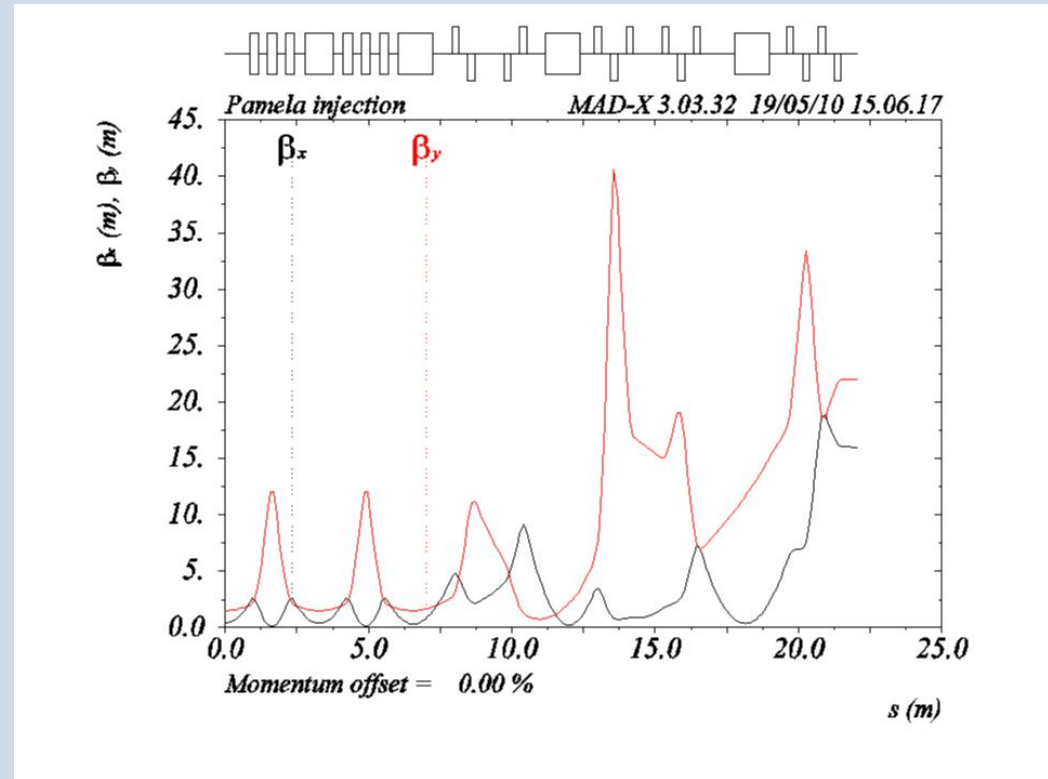
IH structure: shown, TE₁₁₀, Beta=0.1

CH structure: inter-digital fingers rotated by 90 deg., TE₂₁₀, Beta=0.1 to 0.5

Injection into the ring

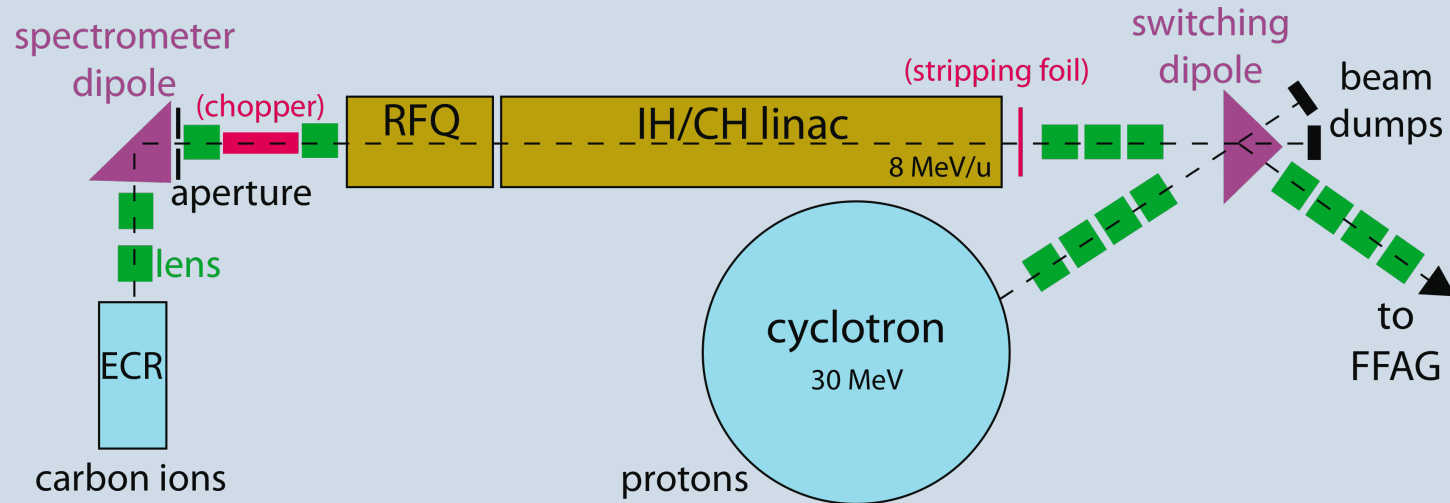


A possible layout of cyclotron inside the first ring



Beta functions of injection line

Injector and Ion Sources



- Pamela injection system is under development and substantial progress has been made
- The specification for PAMELA operation is compatible with C+6 intensities
- Detailed matching of beam from 30 MeV proton cyclotron has been studied.
- Space Charge is not an issue.
- Work on the RFQ is progressing well.
- Work on IH/CH structure, progressing.

Lattice Design

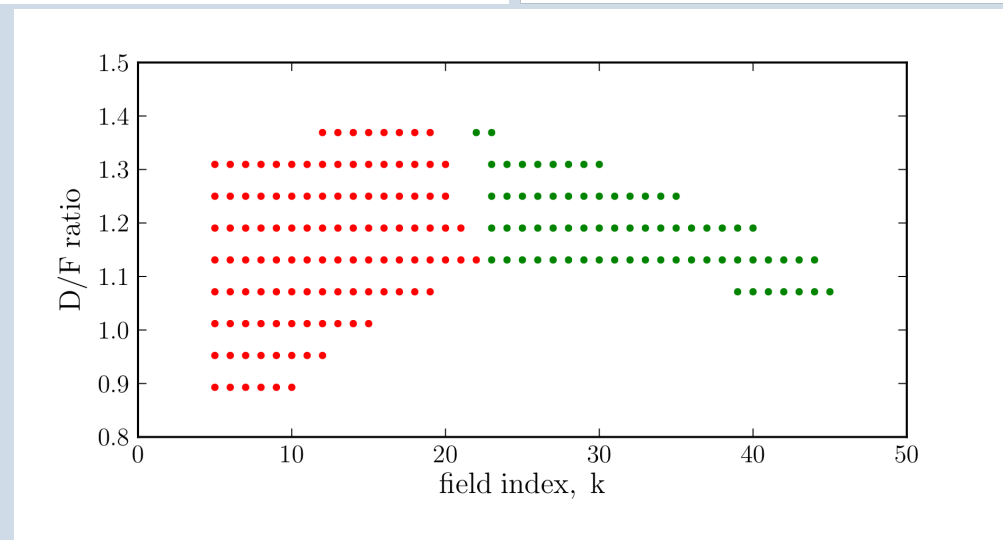
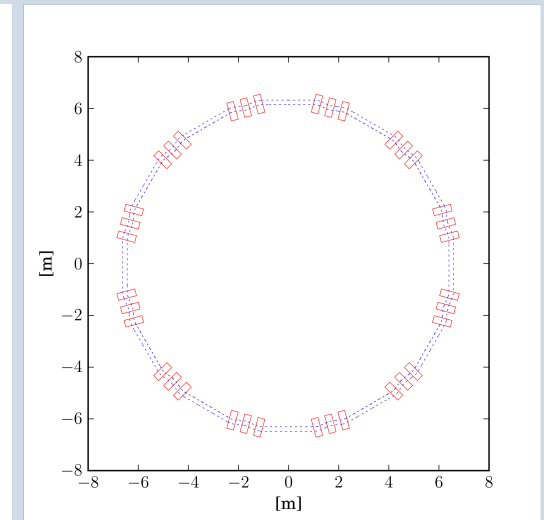
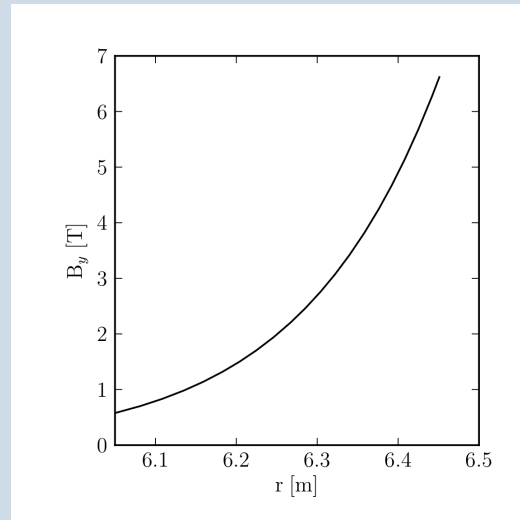
Aim: Minimise tune variation, retain small orbit excursion + hopefully increase long drift section.

Start with scaling FFAG, FDF focusing

Break scaling law

1. Truncate expansion of scaling law
2. Make magnets rectangular
3. Align on straight line

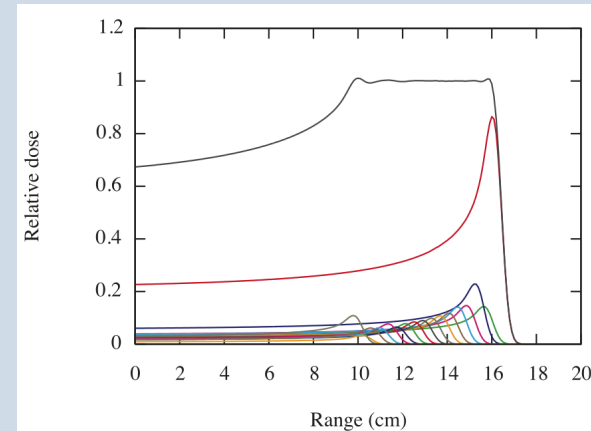
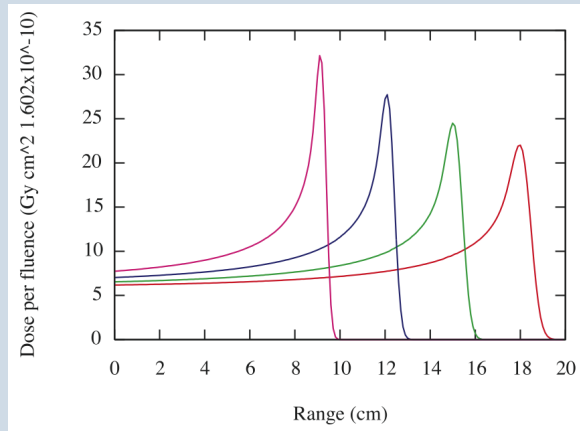
Use 2nd stability region of Hill's equation



Lattice Design – Energies/rigidities

- 2 ring solution
- Could be concentric to reduce footprint

Particle	H+			C6+				
	1 inj	1 ref	1 extr	1 inj	1 ref	1 extr 2 inj	2 ref	2 extr
Kin. En./u [MeV]	30.95	118.38	250	7.8394	30.977	68.357	208.749	400
Bp [Tm]	0.811	1.621	2.432	0.811	1.621	2.432	4.401	6.370



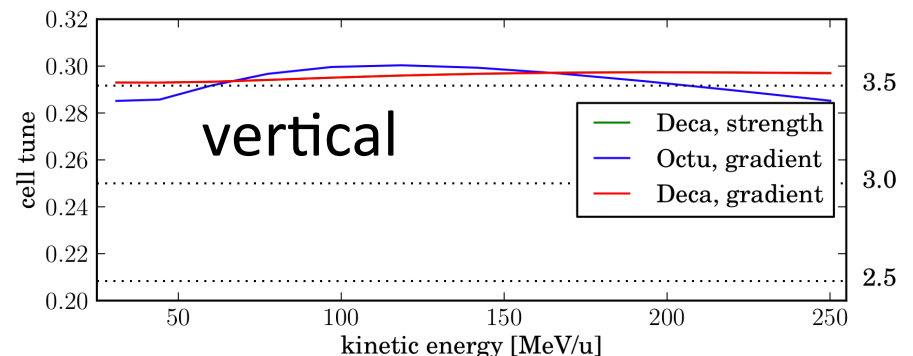
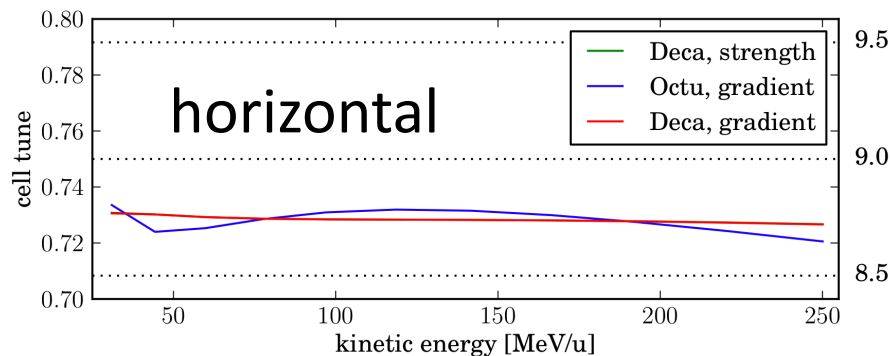
Lattice Design

	Ring 1	Ring 2
Mean Radius [m]	6.251	9.3
Cells	12	12
Packing factor	0.48	0.65
Field index, k	36.721	42
Magnet length [m]	0.3144	0.6330
Orbit exc. [m]	0.1760	0.217 (400 MeV/u) 0.237 (430 MeV/u)
Bore size [m]	~0.24	~0.35

Lattice Performance

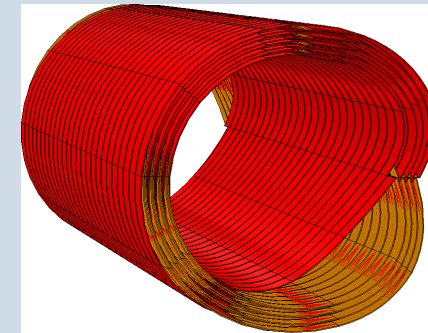
For both the proton and carbon rings:

- Not sensitive to alignment errors
- Total machine tunes within half an integer – no major resonance crossing
- Dynamic aperture $> 50 \pi$ mm mrad (normalised)
- Meets all the requirements



Magnet Design

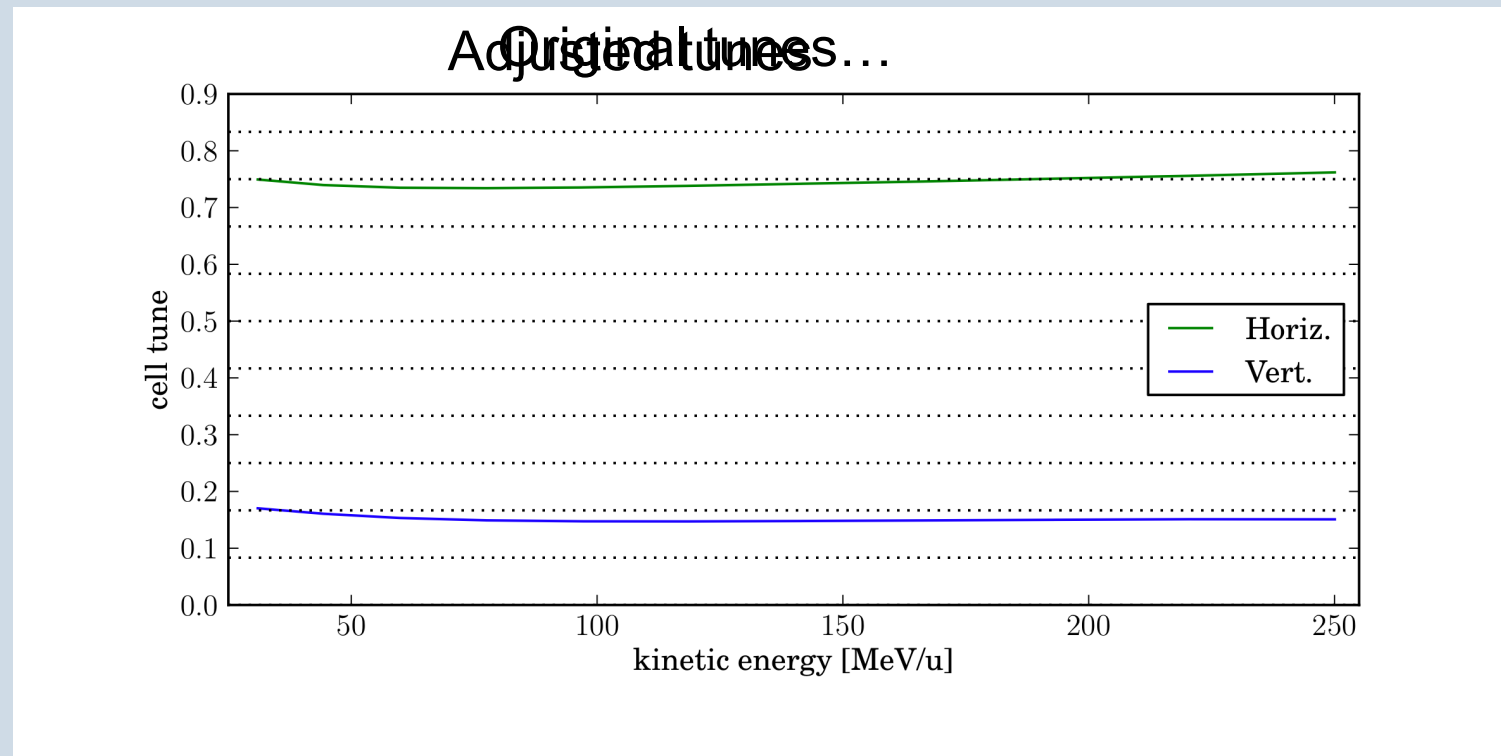
- Magnet Technology Challenges
 - Length restriction
 - Maximum field (4.25T)
 - Combined function magnet (up to decapole)
 - Required bore (>250 mm)
 - Field quality: better than 1×10^{-3}
- Approach: Double-helix coils



Combined function magnet
56.7% Dipole
30.6% Quadrupole
9.7% Sextupole
2.5% Octupole
0.5% Decapole

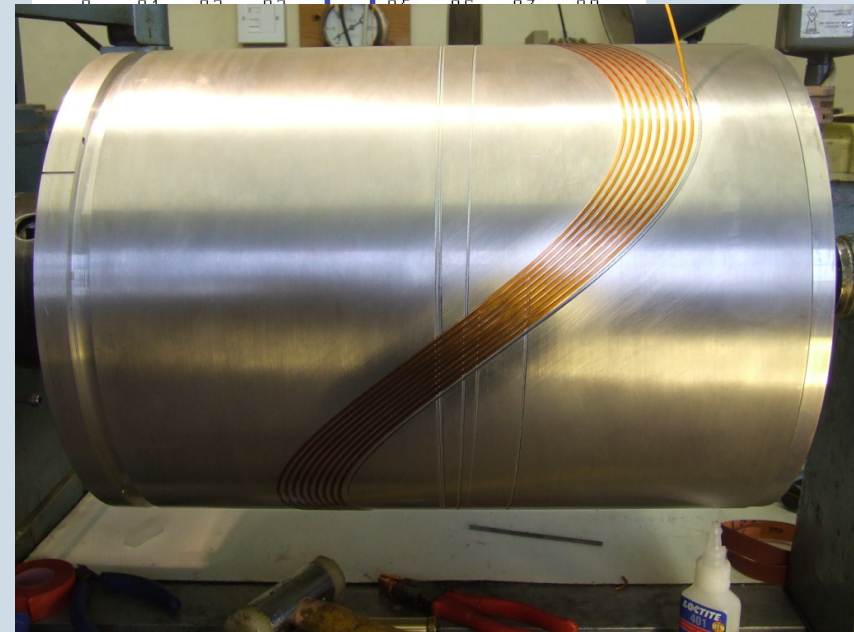
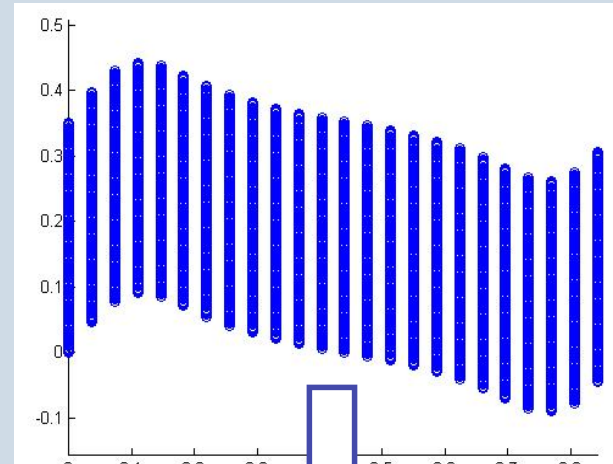
Magnet Design – 3D tracking

- Tracking: Unwanted field components
 - Patent Nov. 2009
- 3D field maps have been tracked in ZGOUBI.

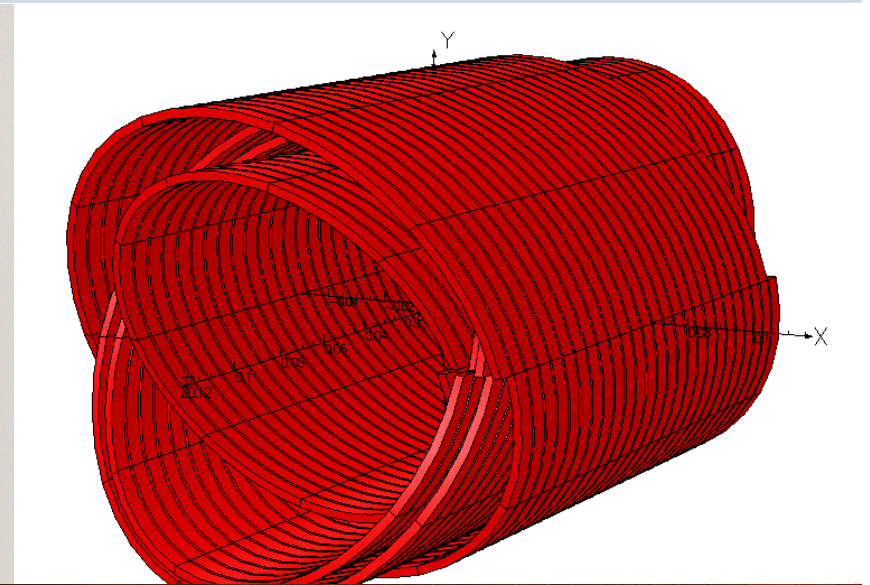
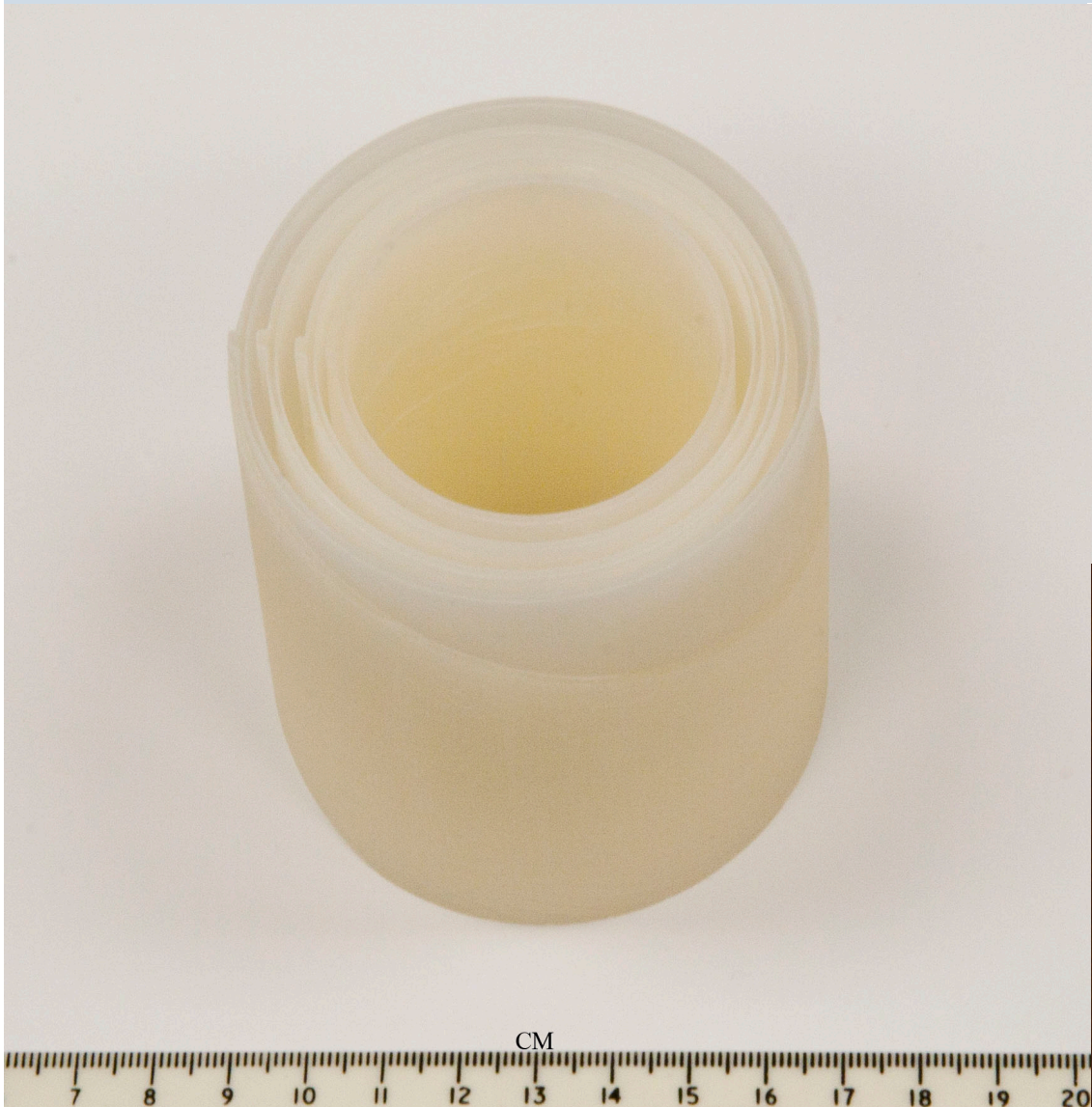


Magnet Design

- Aim: scalable manufacturing process
 - Grooves in flat sheet
 - Precision rolling
- Alignment system
 - Alignment pins
 - Key system
- Photo etching
- First quotations
- Neil Bliss, Shrikant Pattalwar, Thomas Jones, Jonathan Strachan, Holger Witte

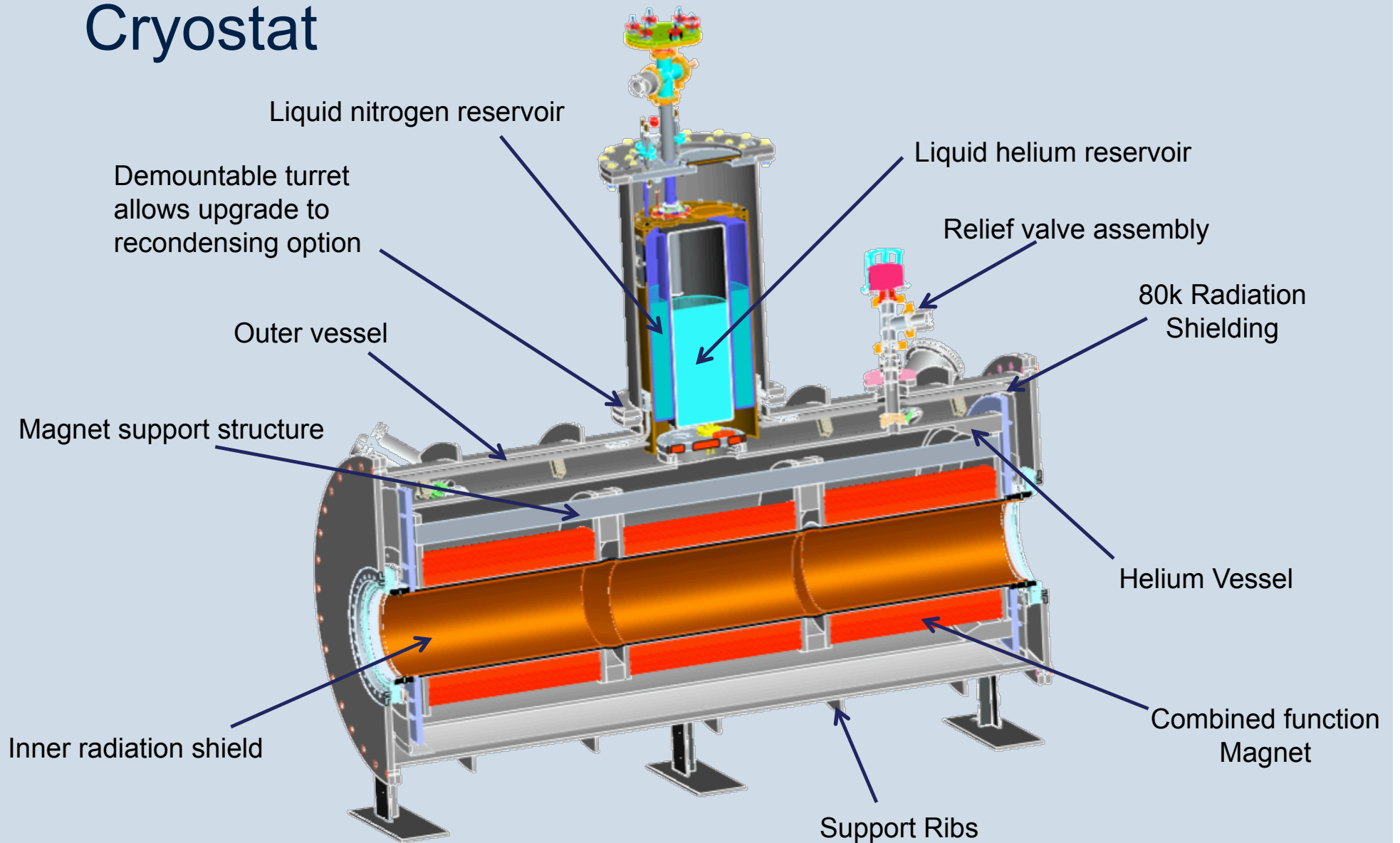


Proposal: Helical Test Coil



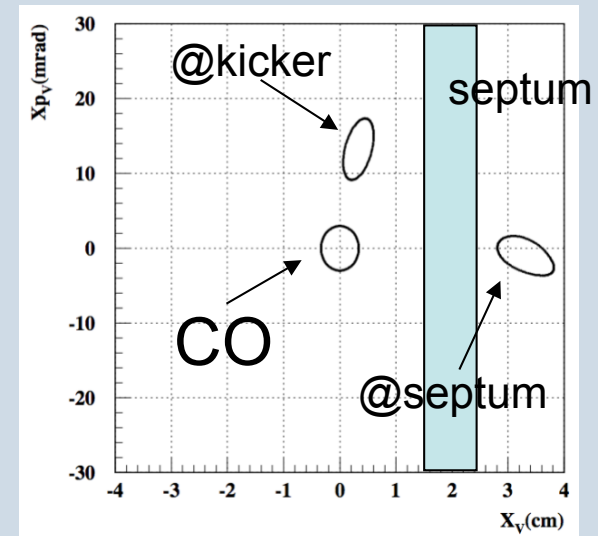
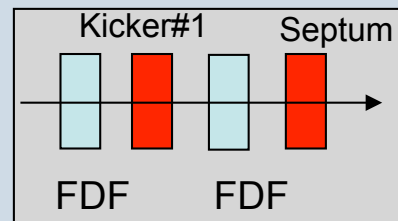
Rapid prototyping model – photo (27/10/10, 11:53pm)

Cryostat



Injection/Extraction

- Extraction kicker proton ring = injection kicker carbon
- Vertical injection & extraction

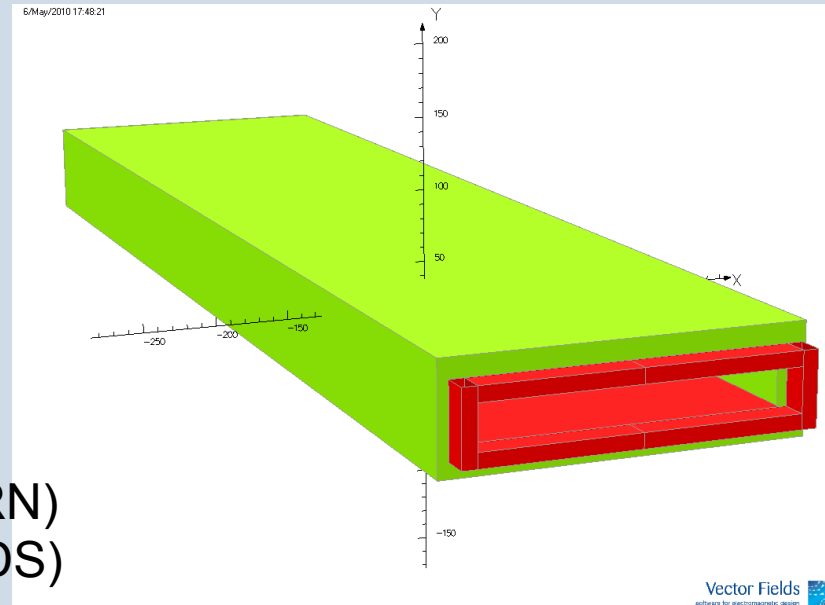


3D model kicker for proton lattice

- Arbitrary ferrite ($B_{sat}=300$ mT)
- Length: 1 m
- Current sheets: 1 mm thickness
- Current densities:
 - Carbon: 167 A/mm²
 - Proton: 55.55 A/mm²
- Magnetic Energy 16/150 J

PFN

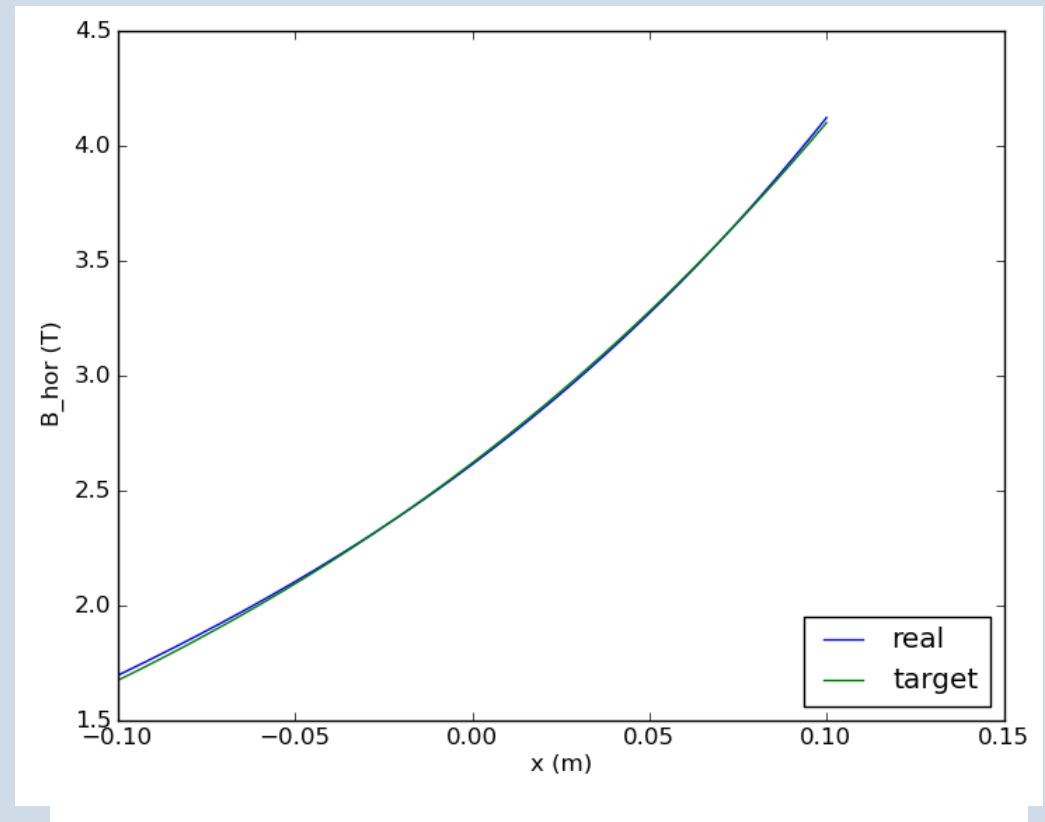
- Conceptual design (approved by CERN)
- Module concept (PAMELA, PRISM, IDS)



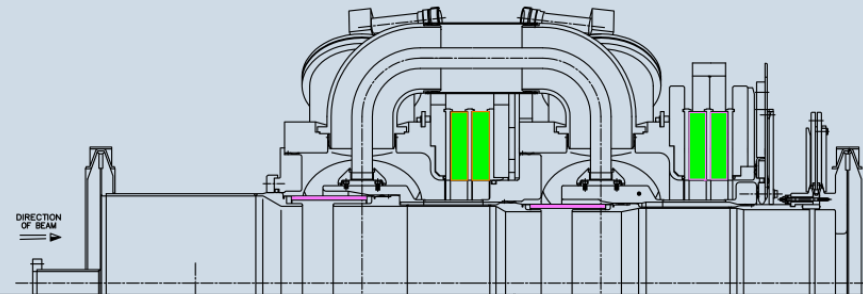
Vector Fields
software for electromagnetic design

Proton lattice septum

- Challenges
 - Large aperture
 - Stray field
 - 4T peak field required
 - Variable energy extraction
 - Field needs to vary
- Superconducting FFAG septum
 - Nb₃Sn



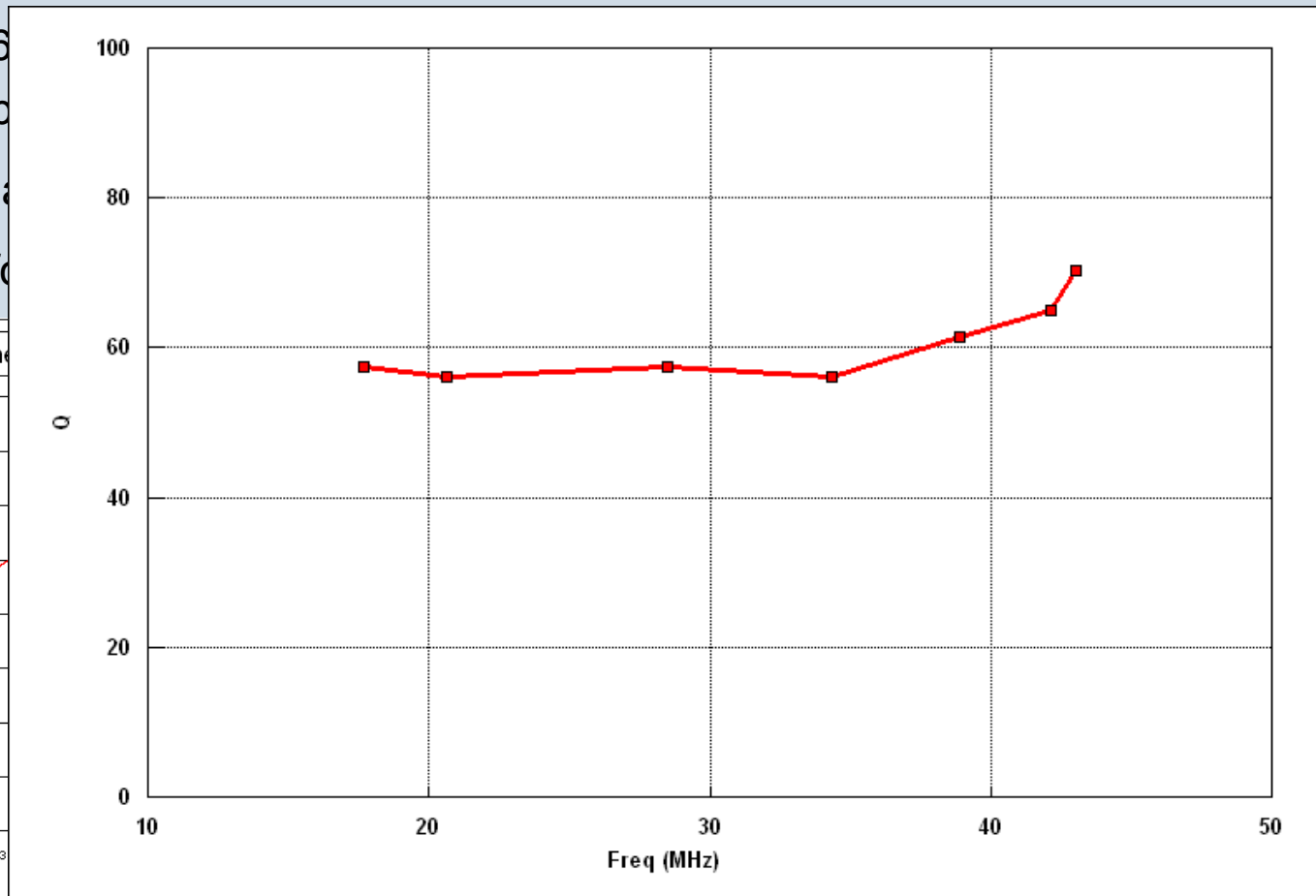
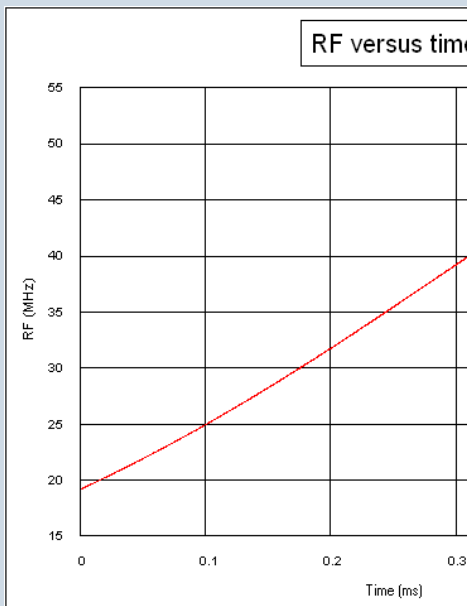
RF Design



	RING 1 Protons	RING 1 C6+	RING 2 C6+
Harmonic	10	17	10
Low rf (MHz)	19.16	16.69	19.21
High rf (MHz)	45.64	45.80	39.10
Frequency swing	2.446	2.818	2.035
Voltage per gap	6-15 kV	6-15 kV	6-15 kV
No. of 2 gap cavs	8	8	8
Voltage per turn	96-240 kV	96-240 kV	96-240 kV
Accel. time	0.4 ms	0.44 ms	1.7 ms

RF Design

- ASSUMING $Q \sim 60$
- RF Power per gap
- RF Power per 2 gaps
- Mean RF Power for



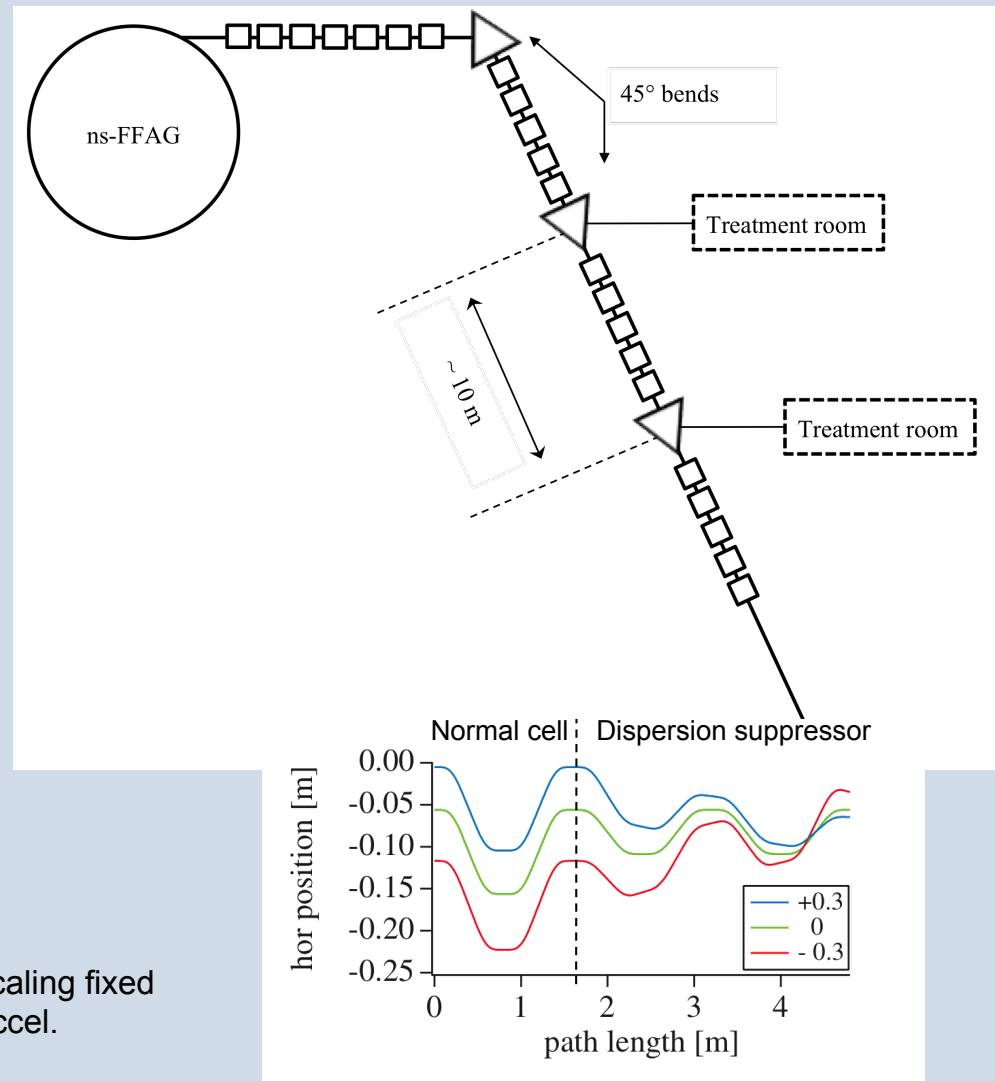
Other ideas: Harmonic Number Jump systems (HNJ), Induction Cavities, Magnetic Alloy loaded cavities (MA), Drift tubes with ferrite resonators, Multiple fixed frequency cavities...

Beam Transport

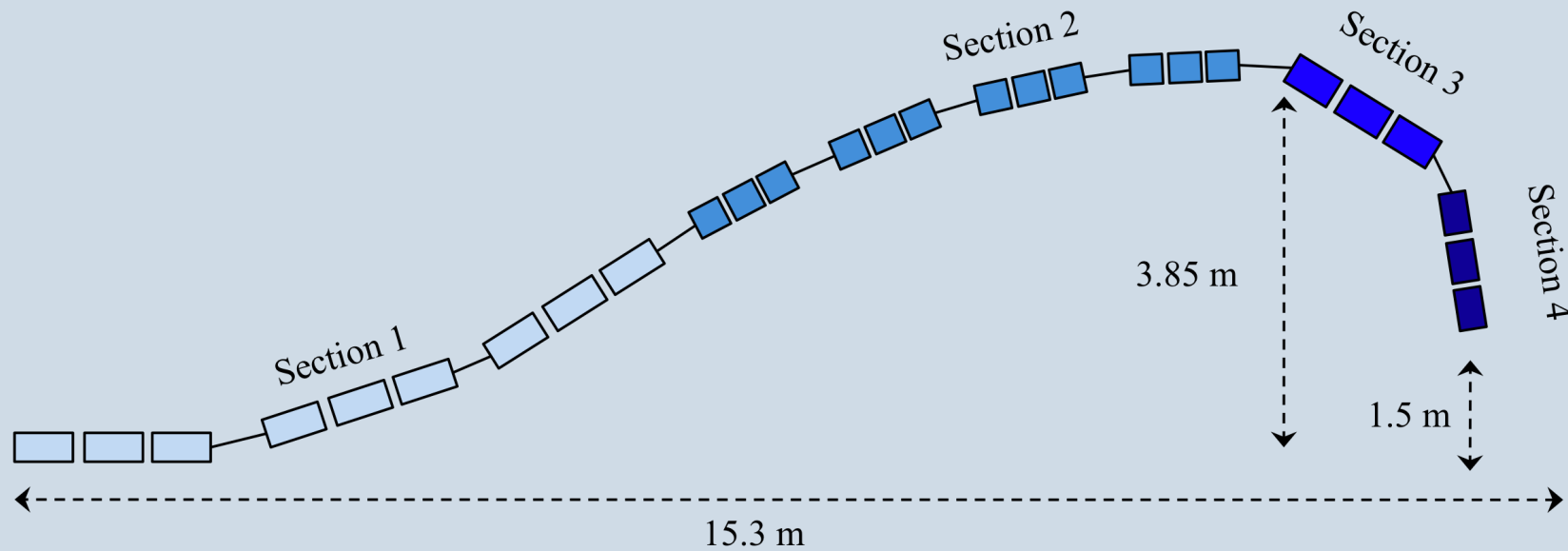
- Many options available
 - Slowest part of system will be magnet changes for scanning & any physical movement – want to minimise
 - Hope to have full FFAG transport & gantry
- FDDF configuration
- Repeated cell structure is 1.6m in length

- Also: dispersion suppressor sections

See: S. Machida, R. Fenning, “Beam transport line with scaling fixed field alternating gradient type magnets”, Phys. Rev. ST. Accel. Beams, **13**, 084001 (2010).

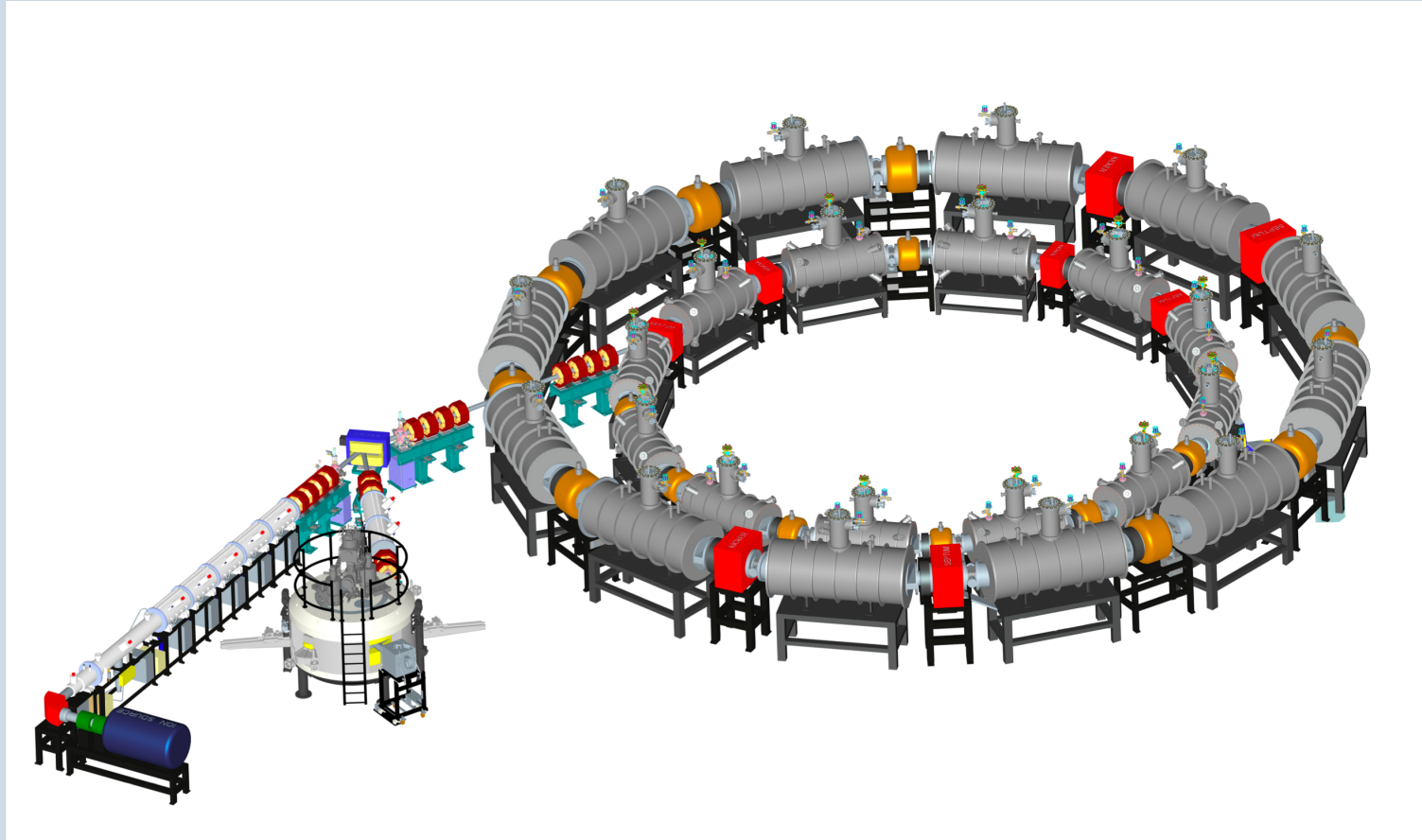


Treatment Gantry



- Ongoing work – initial design by R. Fenning for proton gantry
- Lots of ideas – discussions welcome! (T.Yokoi's talk)

Layout ?



Where are we now?

- Final Design Review was October 4-7th 2010, Oxford
- Final design report being written (due January 2011)
- Need prototyping of:
 - Main ring magnets, kicker and septum magnets
 - RF
 - Ion source
 - Funds/collaborators sought!
- PTCRi – research: optimise treatment & minimise damage

Thanks for your attention.

Oxford (JAI, Gray, PTCRi)

John Cobb , Bleddyn Jones, Ken Peach,
Suzie Sheehy, Holger Witte· Takeichiro
Yokoi, Mark Hill, Boris Vojnovic + others

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Neil Marks· Shinji Machida· Peter
McIntosh, Chris Prior, Susan Smith

Please refer to the forthcoming PAMELA Design
Report for detailed information.